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## Non-enzymatic hydrogen peroxide detection using gold nanoclusters-modified phosphorus incorporated tetrahedral amorphous carbon electrodes

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#### ABSTRACT

Sensitive electrochemical electrodes for hydrogen peroxide  $(H_2O_2)$  detection were developed using gold nanoclusters (NCs) to modify phosphorus incorporated tetrahedral amorphous carbon films (ta-C:P/Au). Au oxide covered Au NCs were electrodeposited on ta-C:P surfaces, and the size of  $Au/AuO_x$  NCs ranged between 50 nm and 91 nm, depending on the deposition time. The ta-C:P/Au electrodes exhibited higher electrocatalytic activity towards  $H_2O_2$  oxidation compared to ta-C:P electrodes. This is due to the three-dimensional island structure of  $Au/AuO_x$  NCs, which accelerates electron exchange between ta-C:P and  $H_2O_2$  in phosphate buffered solution. We also found that ta-C:P/Au electrodes with  $Au/AuO_x$  NCs of a smaller size and moderate coverage exhibited larger current response to  $H_2O_2$  oxidation. The results obtained from amperometric response curves indicated that the use of  $Au/AuO_x$  NCs as microelectrodes directly favored  $H_2O_2$  oxidation through hemispherical diffusion. The linear detection range of  $H_2O_2$  at the non-enzymatic ta-C:P/Au electrodes was identified to be between  $0.2~\mu$ M and 1 mM with a detection limit of 80 nM under optimized conditions. These ta-C:P/Au electrodes have potential applications in  $H_2O_2$  sensing due to their high sensitivity, fast response and long-term stability.

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#### 1. Introduction

The detection of hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) has attracted considerable attention, particularly in physiological and biomedical studies and in the monitoring of biological processes. This is because H<sub>2</sub>O<sub>2</sub> is a reactive oxygen species and also a by-product of many oxidative biological reactions [1]. Many studies on this subject involved the use of glucose oxidase [2,3]. However, the instability of enzymatic activity, due to factors such as temperature, pH and oxygen, restricts the use of enzyme-based sensors [4]. Thus, we propose using a non-enzymatic electrode for H<sub>2</sub>O<sub>2</sub> detection. Carbon materials are regarded to be superior to noble metals due to their low cost, wide potential window and relatively inert electrochemistry in both aqueous and non-aqueous media. Thus, they have potential applications in both biological electrochemistry and industrial electrochemistry [5–10]. The properties of carbon those are important to its use as an electrode material depend on its structural and chemical stability and C-C bond hybridization. For example, highly oriented pyrolytic graphite, glassy carbon

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and "graphitized" carbon black composed of sp2 hybridized carbon atoms are usually made under high temperature and pressure, and they have excellent conductivity and electrocatalytic activity. Carbon nanotubes used for electrochemistry are generally in the form of bundles with various sizes, which limits their broad electrochemical application as a single nanoelectrode [6]. Diamond offers distinct properties compared to the "classical" carbon materials (graphite, glassy carbon, and carbon black) and has attracted considerable interest due to its excellent electrochemical properties such as long-term stability, chemical inertness, wide potential window and low background current [7,9-11]. Diamond-like carbon (DLC) or tetrahedral amorphous carbon (ta-C) film is a disordered material consisting of sp<sup>2</sup> and sp<sup>3</sup> hybridized carbon atoms. The sp<sup>3</sup> fraction of ta-C film made by a filtered cathodic vacuum arc system may be as high as 85-90%. The ta-C films are therefore nearly completely sp<sup>3</sup> hybridized with the tetrahedral bonding of diamond and show comparatively high hardness, excellent biocompatibility, chemical inertness, low friction and wear, and high corrosion resistance [12]. Similar to diamond, ta-C film has a large electrical resistivity ( $10^6$ – $10^8 \Omega$  cm) and usually requires impurity doping to provide sufficient conductivity for electrochemistry. When ta-C or DLC films are doped with nitrogen (ta-C:N), phosphorus (ta-C:P) or Ni (DLC:Ni), they have been shown to be inexpensive, easily fabricated and reproducible materials. These conductive carbon films possess low double layer capacitance, a large potential

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window, low background current, stability in challenging environments, comparative electrocatalysis and high resistance to product adsorption and do not require a non-activation treatment of the electrode surface by polishing, heating or laser activation. With ambient temperature growth on virtually any substrate and smooth surfaces, doped ta-C or DLC films exhibit many advantages over the difficult-to-nucleate, high-temperature growth boron-doped diamond (BDD) films and "classical" carbon materials and are regarded as an appropriate material for electroanalytical applications [5,8,12–20].

However, the electrocatalytic activity of doped ta-C electrodes for H<sub>2</sub>O<sub>2</sub> electro-oxidation is still limited. Metal nanoparticles (NPs) or nanoclusters (NCs), with large surface areas and good electronic properties, show good performance in accumulating charge and in improving the electrochemical response of electrodes in electrochemical sensors and biosensors [21-24]. These metal NPs or NCs, such as Au NPs or NCs, may be partially oxidized in aqueous media [25], and the oxidation products often act as the mediators for the reduction and oxidation of dissolved species in solution [26,27]. Metallic modification of carbon electrodes has been carried out to improve the electrocatalytic activity for H<sub>2</sub>O<sub>2</sub> oxidation in the past few years. For example, You et al. developed a H<sub>2</sub>O<sub>2</sub> detector using a graphite-like carbon film electrode containing 6.5% platinum NPs [28]. Ivandini et al. fabricated Pt-modified diamond electrodes by implantation method to oxidize H<sub>2</sub>O<sub>2</sub> [29]. Chikae et al. fabricated Au and Pt NPs on screen-printed carbon strips using an electrodeposition process and confirmed the electrocatalytic activities of the electrodes in H<sub>2</sub>O<sub>2</sub> oxidation [30]. Hrapovic et al. reported the enhanced activity of Pt NPs modified carbon nanotubes towards H<sub>2</sub>O<sub>2</sub> oxidation or reduction due to the catalytic action of Pt NPs [31]. To our knowledge, there were few reports on H<sub>2</sub>O<sub>2</sub> oxidation with metal NPs- or NCs-modified conductive ta-C electrodes. In this paper, Au NCs-modified ta-C:P (ta-C:P/Au) films were fabricated and the Au deposits were characterized by scanning electron microscopy (SEM). The capability of ta-C:P/Au films as analytical electrodes for H<sub>2</sub>O<sub>2</sub> detection was investigated by voltammetric and amperometric methods. The kinetics of H<sub>2</sub>O<sub>2</sub> oxidation at ta-C:P/Au electrodes was also examined in detail.

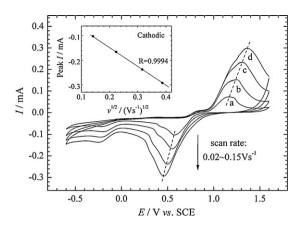
#### 2. Experimental

#### 2.1. Reagents

 $H_2O_2$  solution (30%) and  $HAuCl_4\cdot 3H_2O$  (purity 99.99%) were supplied by Sigma (USA). All other chemicals were of analytical grade. Water was obtained from a Millipore Q purification system (resistivity > 18  $M\Omega$  cm). 0.2 M phosphate buffered solutions (PBS, pH = 5.0–10.0) were prepared by combining appropriate volumes of 0.2 M  $NaH_2PO_4$  and 0.2 M  $Na_2HPO_4$  solutions.

#### 2.2. Preparation of ta-C:P/Au electrodes

Using a filtered cathodic vacuum arc system with 10-sccm phosphine (purity 99.9999%) as the dopant source, 80-nm ta-C:P films were deposited on p-type silicon wafers ( $\rho$  = 0.01–0.02  $\Omega$  cm) [14]. Au NCs were electrodeposited on as-prepared ta-C:P surfaces in a 0.1 M  $\rm H_3BO_4$  solution containing 0.5 mM HAuCl $_4$  (the pH of the solution was adjusted to 1.5 with dense  $\rm H_2SO_4$ ) using an electrochemical workstation (CHI 660A, China) [32]. The potential was scanned from 0.85 V to -0.05 V (vs. saturated calomel electrode (SCE)) and back to 0.85 V for 20 s, 180 s, 360 s and 720 s at a scan rate of 0.02 V s $^{-1}$  under nitrogen bubbling conditions. These ta-C:P/Au samples were correspondingly labeled as ta-C:P/Au $_1$  to ta-C:P/Au $_4$  as the deposition time increased from 20 s to 720 s. The three-electrode system consisted of either a ta-C:P or a ta-C:P/Au working



**Fig. 1.** Cyclic voltammograms of the ta-C:P/Au<sub>1</sub> electrode in a 0.1 M H<sub>2</sub>SO<sub>4</sub> solution at different scan rates. Inset is the dependence of the peak current of Au reduction on the square root of the scan rate.

electrode, a SCE reference electrode and a Pt foil counter electrode. The edges and back of the ta-C:P and ta-C:P/Au electrodes were sealed by an O-ring resin with an apparent geometric surface area ( $A_{\rm g}$ ) of  $0.4\,{\rm cm}^2$ . The as-prepared ta-C:P/Au electrodes were then cycled in  $0.1\,{\rm M}$  H<sub>2</sub>SO<sub>4</sub> solution until a stable voltammogram was achieved, indicating complete cleaning of Au active areas.

#### 2.3. Characterization of ta-C:P/Au electrodes

The composition of the ta-C:P film was measured by X-ray photoemission spectroscopy using a PHI ESCA 5700 spectrometer with an Al K $\alpha$  line (1486.6 eV) as the X-ray source. The content of phosphorus (P/(C+P)) in the ta-C:P film was calculated to be 6.8 at.% from the core level spectra of P 2p and C 1s using the sensitivity factors of the instrument [14]. The deposition process of Au was analyzed by cyclic voltammetry in a 0.1 M H<sub>2</sub>SO<sub>4</sub> solution at different scan rates. Au NCs were examined using a Hitachi S4800 SEM. The electrochemical behavior of the  $Fe(CN)_6^{3-/4-}$ redox couple at ta-C:P and ta-C:P/Au electrodes were investigated in a 5 mM  $K_3$ Fe(CN)<sub>6</sub> and 1 M KCl solution at 0.02 V s<sup>-1</sup>.  $H_2O_2$ detection using ta-C:P and ta-C:P/Au electrodes was performed in 0.2 M PBS with different pHs using the three-electrode system described above. In steady-state amperometric experiments, an optimal potential was selected with a stirring rate of 200 rpm, and the current-time curves were recorded after a constant background current was established. Electrolyte solutions were purged with high-purity nitrogen during electrochemical experiments. The kinetics of H<sub>2</sub>O<sub>2</sub> oxidation at ta-C:P and ta-C:P/Au electrodes was estimated by cyclic voltammetry and amperometric measurement. All electrochemical experiments were carried out at 25 °C using a thermostated water jacket.

#### 3. Results and discussion

#### 3.1. Characterization of Au NCs

Fig. 1 shows the cyclic voltammograms (CVs) of the ta-C:P/Au<sub>1</sub> electrode in a 0.1 M  $\rm H_2SO_4$  solution at different scan rates. A reduction peak of Au was observed at about 0.58 V in the negative scan of Curve a, and the peak at -0.18 V was due to the reduction of hydrogen ions to hydrogen atoms [33]. The peak at 1.16 V on the returning curve was verified to be the oxidation peak of Au deposited on the ta-C:P surface. Furthermore, the reduction peak and oxidation peak of Au shifted cathodically and anodically, respectively, with increasing sweep rates. The linear relationship between the reduction peak current and the square root of sweep rate,  $\nu$  (correlation

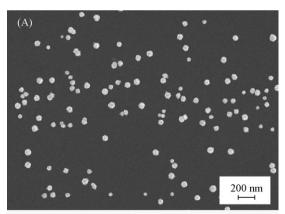
**Table 1**Parameters of ta-C:P/Au electrodes obtained from SEM and voltammetry analyses. The related error for all values is less than 5%.

Sample	A <sub>Au</sub> (cm <sup>2</sup> )	Diameter of Au/AuO <sub>x</sub> NCs (nm)	Density of Au/AuO <sub>x</sub> NCs (units cm <sup>-2</sup> )	Θ	$\Theta_{\mathrm{R}}$	A <sub>U</sub> (cm <sup>2</sup> )	$\Gamma$ (mol cm $^{-2}$ )	$\Delta E_{\rm p} \left( {\sf V} \right)$	$i_{ m p}^{ m ox}/i_{ m p}^{ m red}$
ta-C:P/Au <sub>1</sub>	0.08	50.1	$2.3 \times 10^{9}$	0.045	0.040	0.384	$2.76\times10^{-10}$	0.076	0.94
ta-C:P/Au <sub>2</sub>	0.15	51.7	$5.9 \times 10^9$	0.124	0.120	0.352	$5.20 \times 10^{-10}$	0.066	0.97
ta-C:P/Au <sub>3</sub>	0.23	58.7	$5.1 \times 10^9$	0.138	0.130	0.348	$7.94 \times 10^{-10}$	0.063	0.98
ta-C:P/Au <sub>4</sub>	0.35	90.1	$4.0 \times 10^9$	0.255	0.225	0.310	$1.21\times10^{-9}$	0.063	0.99

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coefficient, R = 0.9994) indicated that the reduction process of Au was diffusion-controlled (the inset in Fig. 1). The Au oxide formed during the position sweep covered the surface of Au NCs, and could serve as a mediator, providing electrocatalytic activity together with Au [25–27]. The real surface area of Au loading ( $A_{Au}$ ) can be estimated from the charge consumed in the reduction of the surface oxide monolayer of Au between 0 V and 0.9 V in the cathodic scan, in N<sub>2</sub>-saturated 0.1 M H<sub>2</sub>SO<sub>4</sub> ( $\nu$  = 0.1 V s<sup>-1</sup>). The reported value of 400  $\mu$ C cm<sup>-2</sup> [34,35] was used. The calculation results shown in Table 1 indicate that  $A_{Au}$  increases with longer deposition time.

The SEM image of the ta-C:P/Au $_2$  electrode shown in Fig. 2A confirms the uniformly discrete nature of Au/AuO $_X$  NCs on a smooth ta-C:P surface. The average diameters of Au/AuO $_X$  NCs for different ta-C:P/Au electrodes were predicted from SEM images using an image analysis software. Results show that the size of Au/AuO $_X$  NCs, prepared at 20 s, ranged between 13.8 nm and 74.3 nm with a mean value of 50.1 nm. After 180 s of electrodeposition, the size of Au/AuO $_X$  NCs varied in a larger range (12.5–75.1 nm) with a 51.7-nm average (Fig. 2A). With deposition time increasing to 360 s and 720 s, the average diameters of Au/AuO $_X$  NCs increased to 58.7 nm and 90.1 nm, respectively. Larger-sized NCs with three-dimensional island structures were also formed after long deposition times (Fig. 2B). These clusters hinted that the



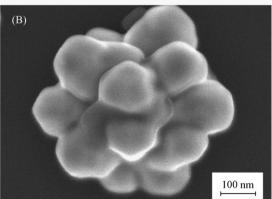


Fig. 2. SEM images of (A) ta-C:P/Au<sub>2</sub> and (B) Au/AuO<sub>x</sub> NC.

growth of some Au sites occurred around the Au seeds deposited previously. The densities of Au/AuO<sub>x</sub> NCs on ta-C:P surfaces were estimated from the SEM images and listed in Table 1. It is clear that the dispersion of Au/AuO<sub>x</sub> NCs, which varies in the range of  $10^9$  units cm<sup>-2</sup> geometrical surface area, strongly depends on the deposition time. Smaller NCs tended to merge and form larger ones due to the overlap of these NCs after long deposition times. This could result in a decrease in the density of Au/AuO<sub>x</sub> NCs. According to the theory of Davies et al. [36], the global coverage of Au/AuO<sub>x</sub> NCs,  $\Theta$ , can be estimated by using an approximation of monolayer distribution of the NCs:

$$\Theta = \frac{\pi R_{\rm b}^2 N_{\rm gold}}{A_{\rm g}},\tag{1}$$

where  $R_b$  is the mean radius of Au NCs and  $N_{gold}$  is the number of Au NCs deposited on the ta-C:P surface with an area of  $A_g$ . The actual area of "uncovered" electrode  $A_U$  is given by:

$$A_{\rm U} = (1 - \Theta_{\rm R})A_{\rm g} \tag{2}$$

where  $\Theta_R$  is the real coverage of Au/AuO<sub>x</sub> NCs and is calculated using the formula:

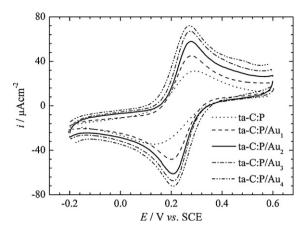
$$\Theta_{\rm R} = 1 - e^{-\Theta} \tag{3}$$

Therefore, the real area of ta-C:P/Au electrodes can be obtained from  $A_{Au}$  and  $A_U$  and the results are shown in Table 1. The surface coverage of Au/AuO $_{\rm X}$ ,  $\Gamma$  (mol cm $^{-2}$ ), on ta-C:P electrodes can also be determined from the charge (Q) associated with the oxidation of Au deposits by sweeping the potential between 0.9 V and 1.6 V in a N2-saturated 0.1 M H2SO4 solution ( $\nu=0.1$  V s $^{-1}$ ) using the following equation [34,37]:

$$\Gamma = \frac{Q}{nFA_g} \tag{4}$$

where n is the stoichiometric number of electrons involved in the electrode reaction and F is the Faraday constant. The data displayed in Table 1 show that higher Au loading results in a larger size of Au/AuO<sub>x</sub> NCs and a larger coverage of Au NCs on the ta-C:P surfaces.  $\Theta_R$  is calculated to be about 0.225 and  $\Gamma$  is 1.21 nmol cm<sup>-2</sup> after 720 s of deposition. This  $\Gamma$  value is less than the amount of Au in an Au (1 1 1) monolayer surface (2.5 nmol cm<sup>-2</sup>) [34]. A continuous Au film is therefore not formed after 720 s of deposition.

Fig. 3A shows the electrochemical behavior of different electrodes in 5 mM  $\rm K_3Fe(CN)_6$  and 1 M KCl solution at a scan rate of 0.02 V s<sup>-1</sup>. The ta-C:P electrode exhibits a nonreversible behavior with a peak potential difference ( $\Delta E_p$ ) of 0.15 V and peak current density ratio ( $i_p^{ox}/i_p^{red}$ ) of 0.90. Comparably, ta-C:P/Au electrodes possess quasi-reversibility towards the Fe(CN)<sub>6</sub><sup>3-/4-</sup> redox reaction and their catalytic capability is dependent on the Au coverage on the electrode surface, as displayed in Table 1. The results indicate that the reversibility of the ta-C:P/Au electrodes is improved after three-dimensional Au/AuO<sub>x</sub> NCs modification, resulting in an enhancement of electrochemical activity.



**Fig. 3.** Cyclic voltammograms of ta-C:P and ta-C:P/Au electrodes in  $5\,\text{mM}$   $K_3[\text{Fe}(\text{CN})_6]$  and  $1\,\text{M}$  KCl solution at  $0.02\,\text{V}\,\text{s}^{-1}$ .

#### 3.2. H<sub>2</sub>O<sub>2</sub> detection using ta-C:P and ta-C:P/Au electrodes

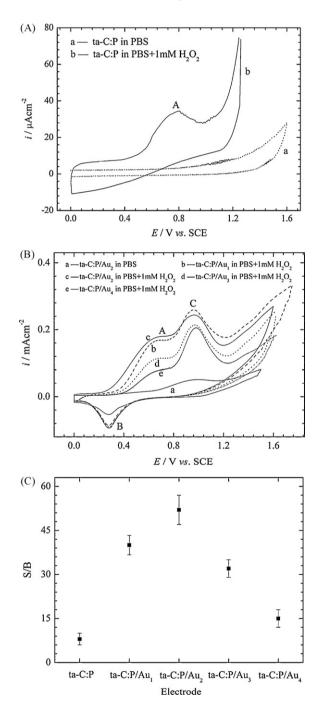
### 3.2.1. Voltammetric responses of $H_2O_2$ on ta-C:P and ta-C:P/Au electrodes

Fig. 4A shows the CVs obtained using the ta-C:P electrode in 0.2 M PBS (pH 7.4) with and without 1 mM of H<sub>2</sub>O<sub>2</sub> at a scan rate of 0.1 V s<sup>-1</sup>. A prominent H<sub>2</sub>O<sub>2</sub> oxidation peak (Peak A) was observed at  $0.78\pm0.08\,V$  (Curve b). The response current of  $H_2O_2$ obtained using ta-C:P may contribute to the catalysis action of active CP sites on the ta-C:P surface [14]. Fig. 4B shows the CVs of ta-C:P/Au electrodes, with different sizes of Au/AuO<sub>x</sub> NCs deposited on them, in 0.2 M PBS (pH 7.4) with 1 mM H<sub>2</sub>O<sub>2</sub> at a scan rate of  $0.1\,\mathrm{V}\,\mathrm{s}^{-1}$ . The two peaks, Peak B at  $0.28\,\mathrm{V}$  and Peak C at  $0.96\,\mathrm{V}$ , observed at the ta-C:P/Au<sub>2</sub> electrode in pure PBS, were attributed to the reduction and oxidation peaks of Au deposited on the ta-C:P surface (Curve a). The catalytic current density obtained at the ta-C:P/Au electrodes (Curves b-e) was 3-6 times higher than that obtained at the ta-C:P electrode upon H<sub>2</sub>O<sub>2</sub> oxidation. Peaks A obtained at the ta-C:P/Au electrodes shifted to  $0.67 \pm 0.06 \, \text{V}$ , which is 0.1 V lower than that obtained at the ta-C:P electrode. The lower oxidation potential and higher current density obtained at the ta-C:P/Au electrodes revealed their higher catalytic abilities towards H<sub>2</sub>O<sub>2</sub> oxidation compared to ta-C:P electrodes. This is because the three-dimensional Au/AuO<sub>x</sub> NCs accelerate the electron exchange between ta-C:P electrodes and H<sub>2</sub>O<sub>2</sub> in aqueous solution. Moreover, the current density of H<sub>2</sub>O<sub>2</sub> oxidation depends on the size of Au/AuO<sub>x</sub> NCs. When 50.1-nm Au/AuO<sub>x</sub> NCs were deposited on the ta-C:P electrode surface, the real surface area of Au NCs on ta-C:P/Au<sub>1</sub> electrode increased. This was accompanied by an increase in the signal to background (S/B) ratio and a decrease in detection potential for H<sub>2</sub>O<sub>2</sub> oxidation (Fig. 4B and C). Although the greater surface area of the ta-C:P/Au<sub>1</sub> electrode might result in an increase in the background current, the sensitivity of H<sub>2</sub>O<sub>2</sub> detection at the ta-C:P/Au<sub>1</sub> electrode was enhanced by improving the S/B ratio. The Au/AuO<sub>x</sub> NCs can be regarded as microelectrodes, uniformly distributed on the ta-C:P surface and a higher detection current can be obtained at each NC. After 180s of deposition, the size of Au/AuO<sub>x</sub> NCs varied in a wider range with a slight increase in the average diameter. The S/B ratio increased due to the increased real surface area of ta-C:P/Au<sub>2</sub>. Further lengthening of the deposition time improved the growth of Au/AuO<sub>x</sub> NCs and increased the background current, resulting in a decrease in the S/B ratio (Fig. 4C). In an earlier study, Hutton et al. [38] reported that the exchange current density of Pt clusters-modified glassy carbon for hydrogen evolution increased with a decrease in Pt particle size. Jia et al. [39] also found that biosensors fabricated with smaller-sized Au NPs exhibited a larger current response than those prepared with larger-sized

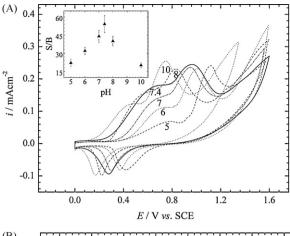
Au NPs. The maximum value of S/B is obtained at a ta-C:P/Au<sub>2</sub> electrode with moderate coverage and thus, it was the chosen electrode for the following voltammetric and amperometric measurements.

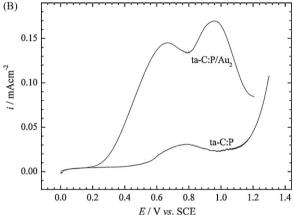
#### 3.2.2. Effect of pH and detection potential

The effect of pH of the measurement solution on the peak current density obtained at the ta-C:P/Au $_2$  electrode was investigated (Fig. 5A), since pH is an important factor in the sensitivity, activity and stability of electrodes. It is interesting to note that the voltammetric waves shift negatively when increasing pH from 5.0 to 10.0. This may be attributed to the increase of negative charge on the ta-C:P/Au $_2$  electrode. The current response to 1 mM H $_2$ O $_2$  obtained



**Fig. 4.** Cyclic voltammograms of (A) ta-C:P and (B) ta-C:P/Au electrodes in 0.2 M PBS (pH 7.4) with and without 1 mM  $H_2O_2$  at 0.1 V  $s^{-1}$ . (C) Signal/background ratios calculated from the cyclic voltammograms of ta-C:P and ta-C:P/Au electrodes in 0.2 M PBS (pH 7.4) with and without 1 mM  $H_2O_2$ .





**Fig. 5.** (A) Cyclic voltammograms of the ta-C:P/Au $_2$  electrode in 1 mM  $H_2O_2$  and 0.2 M PBS at different pH. Inset is the dependence of signal/background ratio on pH at the ta-C:P/Au $_2$  electrode in 0.2 M PBS with 1 mM  $H_2O_2$ . (B) Evolution of current density difference with the change of potential obtained at ta-C:P and ta-C:P/Au $_2$  electrodes in 0.2 M PBS (pH 7.4) with and without 1 mM  $H_2O_2$ .

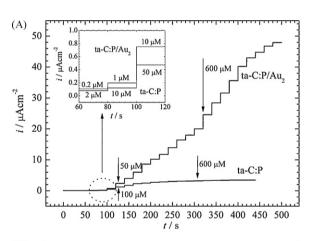
at the ta-C:P/Au<sub>2</sub> electrode increased pronouncedly from pH 5.0 to 7.0, changed slightly in the pH region between 7.0 and 8.0, then decreased when pH was greater than 8.0. According to Hall et al. [40], acidic conditions were likely to hinder the formation of the binding site and could result in protonation, producing inactive sites with higher anodic potential. In addition, the contribution of background current at pH 7.4 was very low, in contrast to those observed at other pH values. The maximum S/B ratio was therefore obtained at pH 7.4 (see inset in Fig. 5A). The effect of pH of the measurement solution on the peak current density obtained at the ta-C:P electrode was similar to that obtained at the ta-C:P/Au<sub>2</sub> electrode. Therefore, both ta-C:P and ta-C:P/Au<sub>2</sub> electrodes are suitable for the detection of H<sub>2</sub>O<sub>2</sub> at pH 7.4.

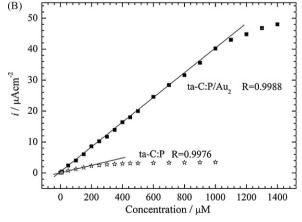
Moreover, the difference in current densities due to change in potential obtained at ta-C:P and ta-C:P/Au $_2$  electrodes in 0.2 M PBS (pH 7.4) with and without 1 mM  $\rm H_2O_2$  was calculated. It can be seen from Fig. 5B that 0.77 V and 0.67 V should be chosen as the optimal measurement potentials for ta-C:P and ta-C:P/Au $_2$  electrodes to avoid interference from Au oxidation and  $\rm O_2$  evolution.

## 3.2.3. Amperometric responses of $H_2O_2$ at ta-C:P and ta-C:P/Au electrodes

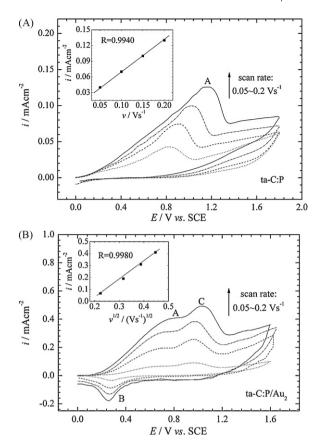
Fig. 6A shows typical amperometric response curves of  $H_2O_2$  oxidation at ta-C:P and ta-C:P/Au<sub>2</sub> electrodes using the above optimum conditions (0.77 V detection potential for ta-C:P and 0.67 V for ta-C:P/Au<sub>2</sub>, 0.2 M PBS at pH 7.4) with successive increments of  $H_2O_2$ , of various volumes and concentrations, in 10 mL PBS. The electrode responses achieved steady-state signals within 8 s. The

linear characteristics of the electrodes for H<sub>2</sub>O<sub>2</sub> detection can be observed in Fig. 6B. The current density of H<sub>2</sub>O<sub>2</sub> oxidation obtained at the ta-C:P electrode was proportional to the H<sub>2</sub>O<sub>2</sub> concentration in the range of 2-200 µM, with a sensitivity (change of current density per unit concentration of  $H_2O_2$ ) of  $48.4 \pm 0.2$  nA cm<sup>-2</sup>/ $\mu$ M (R=0.9976). The detection limit, based on the signal-to-noise ratio (S/N = 3), was estimated to be  $0.5 \pm 0.1 \,\mu\text{M}$ . After modification with Au/AuOx NCs, the current density of H2O2 oxidation obtained at the ta-C:P/Au<sub>2</sub> electrode was linear within a wider concentration range from  $0.2 \,\mu\text{M}$  to  $1 \,\text{mM}$  (R = 0.9988) and had a sensitivity of  $293.8 \pm 0.3 \,\text{nA}\,\text{cm}^{-2}/\mu\text{M}$ . The detection limit at S/N = 3 was calculated to be 80 nM. This value was one order of magnitude lower than that obtained at the ta-C:P electrode under the same conditions, and three orders of magnitude lower than that obtained at DLC electrodes  $(20-30 \,\mu\text{M})$  [8]. When the concentration of  $H_2O_2$  exceeded 1 mM, the current density obtained at the ta-C:P/Au<sub>2</sub> electrode was no longer proportional to the bulk H<sub>2</sub>O<sub>2</sub> concentration. The current density of H<sub>2</sub>O<sub>2</sub> oxidation saturated at a lower concentration of 300 µM at the ta-C:P electrode. This may be explained by the suggestion that maximum electrode response and sensitivity can only be obtained when oxygen gas (a product of H<sub>2</sub>O<sub>2</sub> oxidation) is rapidly removed from the vicinity of the electrode. The postponed diffusion of O<sub>2</sub> from the electrode surface to the solution, and H<sub>2</sub>O<sub>2</sub> from the solution to the electrode surface slows down the reaction rate and affects the kinetics of the overall reaction when a large amount of O2 is created on the electrode surface. As a result, the





**Fig. 6.** (A) Current density–time response of  $H_2O_2$  oxidation obtained at ta-C:P and ta-C:P/Au<sub>2</sub> electrodes with successive addition of various volumes and concentrations  $H_2O_2$  into 10 m.L 0.2 M PBS (pH 7.4). Electrode potential: 0.77 V vs. SCE for ta-C:P and 0.67 V vs. SCE for ta-C:P/Au<sub>2</sub>. The solution was stirred magnetically during measurements. Inset is the magnification of the dashed part. (B) Relation between the current density of  $H_2O_2$  oxidation and the concentration of  $H_2O_2$  obtained at the ta-C:P and ta-C:P/Au<sub>2</sub> electrodes in 0.2 M PBS (pH 7.4).



**Fig. 7.** Cyclic voltammograms of (A) ta-C:P and (B) ta-C:P/ $Au_2$  electrodes in 0.2 M PBS (pH 7.4) with 5 mM  $H_2O_2$  at different scan rates. Inset represents the dependence of peak current density of  $H_2O_2$  oxidation on scan rate or square root of scan rate.

sensitivities of ta-C:P and ta-C:P/Au $_2$  electrodes are lowered. ta-C:P electrodes with smaller surface area tend to be passivated and ineffective in the presence of lower amounts of O $_2$  or H $_2$ O $_2$ . ta-C:P/Au $_2$  electrodes with a larger real surface area and higher ratio of  $A_{Au}$  to real surface area preponderates over ta-C:P electrodes in terms of the higher S/B and S/N ratios, and a lower detection limit can therefore be obtained at this electrode.

#### 3.3. Kinetics of $H_2O_2$ oxidation

The kinetics of  $\rm H_2O_2$  oxidation at ta-C:P and ta-C:P/Au<sub>2</sub> electrodes were estimated by cyclic voltammetry and current–time measurement. Fig. 7 shows the CVs obtained at ta-C:P and ta-C:P/Au<sub>2</sub> electrodes in 0.2 M PBS (pH 7.4), with 5 mM  $\rm H_2O_2$ , at different scan rates. The peak position of  $\rm H_2O_2$  oxidation at the ta-C:P electrode obviously shifted towards the positive direction with increasing scan rate. The peak current density of  $\rm H_2O_2$  oxidation was dependent on the scan rate from 0.05 V s<sup>-1</sup> to 0.2 V s<sup>-1</sup> (R=0.9940). The overall process of  $\rm H_2O_2$  oxidation was therefore a surface-controlled electrode process. Thus, an excellent linear relation between the peak current density of  $\rm H_2O_2$  oxidation and the square root of scan rate (v=0.05–0.2 V s<sup>-1</sup>) with R=0.9980 was obtained at the ta-C:P/Au<sub>2</sub> electrode, demonstrating the speedy reaction kinetics and diffusion-controlled process (Fig. 7B).

Fig. 8A shows the current density–time curves obtained at the ta-C:P/Au<sub>2</sub> electrode in 0.2 M PBS (pH 7.4) with and without 1–5 mM  $\rm H_2O_2$ . According to the theory of diffusion control, the time (t) dependence of the current (I) for linear diffusion at a planar electrode follows Cottrell's equation [41]:

$$I = nFAD_0^{1/2}C_0^*\pi^{-1/2}t^{-1/2},\tag{5}$$

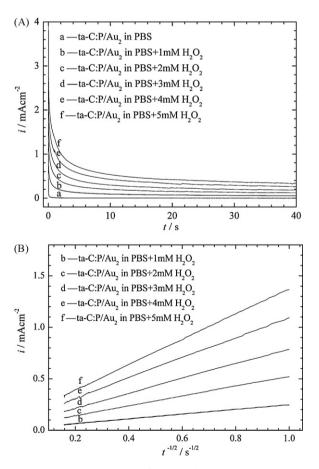
where  $D_0$  is the diffusion coefficient and  $C_0^*$  is the concentration of the active species. The area A may be the geometric surface area or the real surface area of the electrode, depending on measurement time [34]. Similarly, the time dependence of the current for hemispherical diffusion at a microelectrode is described by the following equation:

$$I = nFAD_0C_0^*(\pi^{-1/2}D_0^{-1/2}t^{-1/2} + 4\pi^{-1}r^{-1}),$$
 (6)

where r is the radius of the microelectrode. It can be seen from Fig. 8B that the intercepts of the Cottrell plots are not zero and the slopes are small, indicating that the total current density has a small time-independent component. It can be inferred that the kinetics of  $H_2O_2$  oxidation at the ta-C:P/Au $_2$  electrode is mainly controlled by hemispherical diffusion. The three-dimensional Au/Au $O_x$  NCs not only accelerate the electron exchange between the ta-C:P electrode and  $H_2O_2$  but also directly favors  $H_2O_2$  oxidation as microelectrode arrays on the ta-C:P surface. That is, Au/Au $O_x$  NCs are dispersed on the surface of the ta-C:P electrode in the form of microelectrodes.

#### 3.4. Reproducibility of the ta-C:P/Au electrode

The repeatability of ta-C:P/Au $_2$  electrode is tested. The relative standard deviation of amperometric current responses recorded by 100 injections of 10  $\mu$ L of H $_2$ O $_2$  (1 mM) was found to be 4.5%. The long-term stability of the ta-C:P/Au $_2$  electrode was investigated over a 60-day period. ta-C:P/Au $_2$  electrode was stored at 4  $^{\circ}$ C and measured every 2 days. The electrode's response to H $_2$ O $_2$  oxidation under identical conditions decreased to 85% of the initial response



**Fig. 8.** (A) Amperometric responses of the ta-C:P/Au $_2$  electrode in 0.2 M PBS (pH 7.4) with and without different concentrations of H $_2$ O $_2$ . (B) Cottrell plots obtained at the ta-C:P/Au $_2$  electrode in 0.2 M PBS (pH 7.4) with different concentrations of H $_2$ O $_2$ .

after 2 weeks due to the absence of some  $Au/AuO_x$  NCs. However, the response maintained at a similar level during a 2-month period thereafter, implying the long-term stability of the electrode.

#### 4. Conclusions

Gold NCs-modified, phosphorus incorporated tetrahedral amorphous carbon (ta-C:P/Au) was fabricated using a filtered cathodic vacuum arc process followed by electrodeposition. The real surface area of ta-C:P/Au electrodes modified with Au/AuO<sub>x</sub> NCs increased compared to that of ta-C:P electrodes. The size and coverage of Au/AuO<sub>x</sub> NCs can be adjusted by controlling the deposition time. The Au/AuO<sub>x</sub> NCs significantly improved the electrochemical activity and reversibility of ta-C:P electrodes towards ferricyanide oxidation reaction and provided high catalytic activity towards hydrogen oxidation (H<sub>2</sub>O<sub>2</sub>) oxidation due to the action of threedimensional NCs. The detection limit of H<sub>2</sub>O<sub>2</sub> obtained at the ta-C:P/Au electrode with Au/AuO<sub>x</sub> NCs of small size and moderate coverage was estimated to be 80 nm, which was one order magnitude smaller than that obtained at the ta-C:P electrode under optimal conditions. The results from current density-time measurement indicated that H<sub>2</sub>O<sub>2</sub> oxidation at the ta-C:P/Au electrode was mainly controlled by hemispherical diffusion. Accelerated oxidation of H<sub>2</sub>O<sub>2</sub> was induced by Au/AuO<sub>x</sub> NCs microelectrodes dispersed on ta-C:P surfaces. The successful detection of H<sub>2</sub>O<sub>2</sub> at ta-C:P/Au electrodes implies that the electrodes may be applied as a non-enzymatic H<sub>2</sub>O<sub>2</sub>-based biosensor due to their immediate response, high sensitivity and good reproducibility.

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